BEST AVAILABLE COPY

(12) INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

(19) World Intellectual Property Organization International Bureau



(43) International Publication Date 3 February 2005 (03.02.2005)

PCT

(10) International Publication Number WO 2005/009301 A1

(51) International Patent Classification7:

A61F 2/44

(21) International Application Number:

PCT/US2004/016774

(22) International Filing Date:

24 May 2004 (24.05.2004)

(25) Filing Language:

English

(26) Publication Language:

English

(30) Priority Data:

10/615,417

8 July 2003 (08.07.2003) US

- (71) Applicant (for all designated States except US): ARCHUS ORTHOPEDICS, INC. [US/US]; 8624 - 154th Avenue NE, Redmond, Washington 98052 (US).
- (72) Inventors; and
- (75) Inventors/Applicants (for US only): STINSON, David [US/US]; 15009 NE 195th Street, Woodinville, Washington 98072 (US). JONES, Lawrence [US/US]; 11701 Baca Road, Conifer, Colorado 80433 (US). SCRIBNER, Robert [US/US]; 7042 Quite Retreat Road, Niwot, Colorado 80503 (US). REILEY, Mark [US/US]; 360 Magnolia Avenue, Piedmont, California 94611 (US).
- (74) Agents: SHAY, James et al.; Wilson Sonsini Goodrich & Rosati, 650 Page Mill Road, Palo Alto, CA 94304-1050 (US).

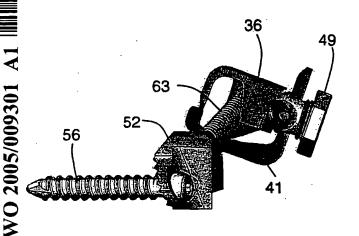
- (81) Designated States (unless otherwise indicated, for every kind of national protection available): AE, AG, AL, AM, AT, AU, AZ, BA, BB, BG, BR, BW, BY, BZ, CA, CH, CN, CO, CR, CU, CZ, DE, DK, DM, DZ, EC, EE, EG, ES, FI, GB, GD, GE, GH, GM, HR, HU, ID, IL, IN, IS, JP, KE, KG, KP, KR, KZ, LC, LK, LR, LS, LT, LU, LV, MA, MD, MG, MK, MN, MW, MX, MZ, NA, NI, NO, NZ, OM, PG, PH, PL, PT, RO, RU, SC, SD, SE, SG, SK, SL, SY, TJ, TM, TN, TR, TT, TZ, UA, UG, US, UZ, VC, VN, YU, ZA, ZM, ZW.
- (84) Designated States (unless otherwise indicated, for every kind of regional protection available): ARIPO (BW, GH, GM, KE, LS, MW, MZ, NA, SD, SL, SZ, TZ, UG, ZM, ZW), Eurasian (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM), European (AT, BE, BG, CH, CY, CZ, DE, DK, EE, ES, FI, FR, GB, GR, HU, IE, IT, LU, MC, NL, PL, PT, RO, SE, SI, SK, TR), OAPI (BF, BJ, CF, CG, CI, CM, GA, GN, GQ, GW, ML, MR, NE, SN, TD, TG).

Published:

with international search report

For two-letter codes and other abbreviations, refer to the "Guidance Notes on Codes and Abbreviations" appearing at the beginning of each regular issue of the PCT Gazette.

(54) Title: PROSTHESES AND TOOLS FOR REPLACEMENT OF NATURAL FACET JOINTS



(57) Abstract: Cephalad and caudal vertebral facet joint prostheses and methods of use are provided. The cephalad prostheses are adapted and configured to be attached to a lamina portion of a vertebra without blocking a pedicle portion of the cephalad vertebra. In some embodiments, the prosthesis is attached with a non-invasive support member, such as a clamp. In other embodiments, a translaminar screw may be used for additional fixation.

BEST AVAILABLE COPY

WO 2005/009301 PCT/US2004/016774

PROSTHESES AND TOOLS FOR REPLACEMENT OF NATURAL FACET JOINTS

Field of the Invention

This invention relates to prostheses for treating various types of spinal pathologies, as well as to methods of treating spinal pathologies.

Background of the Invention

I. VERTEBRAL ANATOMY

As Fig. 1 shows, the human spinal column 10 is comprised of a series of thirty-three stacked vertebrae 12 divided into five regions. The cervical region includes seven vertebrae 12, known as C1-C7. The thoracic region includes twelve vertebrae 12, known as T1-T12. The lumbar region contains five vertebrae 12, known as L1-L5. The sacral region is comprised of five vertebrae 12, known as S1-S5. The coccygeal region contains four vertebrae 12, known as C01-C04.

Fig. 2 shows a normal human lumbar vertebra 12. Although the lumbar vertebrae 12 vary somewhat according to location, they share many features common to most vertebrae 12. Each vertebra 12 includes a vertebral body 14 and posterior elements as follows:

Two short bones, the pedicles 16, extend backward from each side of the vertebral body 14 to form a vertebral arch 18. At the posterior end of each pedicle 16 the vertebral arch 18 flares out into broad plates of bone known as the laminae 20. The laminae 20 fuse with each other to form a spinous process 22. The spinous process 22 serves for muscle and ligamentous attachment. A smooth transition from the pedicles 16 into the laminae 20 is interrupted by the formation of a series of processes.

Two transverse processes 24 thrust out laterally on each side from the junction of the pedicle 16 with the lamina 20. The transverse processes 24 serve as levers for the attachment of muscles to the vertebrae 12. Four articular processes, two superior 26 and two inferior 28, also rise from the junctions of the pedicles 16 and the laminae 20. The superior articular processes 26 are sharp oval plates of bone rising upward on each side from the union of the pedicle 16 with the lamina 20. The inferior processes 28 are oval plates of bone that extend in an inferior direction on each side.

The superior and inferior articular processes 26 and 28 each have a natural bony structure known as a facet. The superior articular facet 30 faces upward or superiorly, while the inferior articular facet 31 faces downward. As Fig. 3 shows, when adjacent (i.e., cephalad and caudal)

vertebrae 12 are aligned, the facets 30 and 31, capped with a smooth articular cartilage, interlock to form a facet joint 32, also known as a zygapophysial joint.

The facet joint 32 is composed of a superior half and an inferior half. The superior half is formed by the vertebral level below the joint 32, and the inferior half is formed by the vertebral level above the joint 32. For example, in the L4-L5 facet joint, the superior portion of the joint is formed by bony structure on the L-5 vertebra (e.g., a superior articular surface and supporting bone on the L-5 vertebra), and the inferior portion of the joint is formed by bony structure on the L-4 vertebra (e.g., an inferior articular surface and supporting bone on the L-4 vertebra).

As also shown in Fig. 3, an intervertebral disc 34 between each pair of vertebrae 12 permits relative movement between vertebrae 12. Thus, the structure and alignment of the vertebrae 12 permit a range of movement of the vertebrae 12 relative to each other.

II. FACET JOINT DYSFUNCTION

Back pain, particularly in the "small of the back", or lumbosacral (L4-S1) region, is a common ailment. In many cases, the pain severely limits a person's functional ability and quality of life. Such pain can result from a variety of spinal pathologies.

Through disease or injury, the laminae, spinous process, articular processes, or facets of one or more vertebrae can become damaged, such that the vertebrae no longer articulate or properly align with each other. This can result in an undesired anatomy, pain or discomfort, and loss of mobility.

For example, the vertebral facet joints can be damaged by either traumatic injury or by various disease processes. These disease processes include osteoarthritis, ankylosing spondylolysis, and degenerative spondylolisthesis. The damage to the facet joints often results in pressure on nerves, also called a "pinched" nerve, or nerve compression or impingement. The result is pain, misaligned anatomy, and a corresponding loss of mobility. Pressure on nerves can also occur without facet joint pathology, e.g., a herniated disc.

One type of conventional treatment of facet joint pathology is spinal stabilization, also known as intervertebral stabilization. Intervertebral stabilization prevents relative motion between the vertebrae. By preventing movement, pain can be reduced. Stabilization can be accomplished by various methods.

One method of stabilization is posterior spinal fusion. Another

method of stabilization is anterior spinal fusion, fixation of any number of vertebrae to stabilize and prevent movement of the vertebrae.

Another type of conventional treatment is decompressive laminectomy. This procedure involves excision of the laminae to relieve compression of nerves.

These traditional treatments are subject to a variety of limitations and varying success rates. Furthermore, none of the described treatments puts the spine in proper alignment or return the spine to a desired anatomy. In addition, stabilization techniques, by holding the vertebrae in a fixed position, permanently limit the relative motion of the vertebrae, altering spine biomechanics.

Summary of the Invention

There is a need for prostheses, installation tools, and methods that overcome the problems and disadvantages associated with current strategies and designs in various treatments for spine pathologies.

The invention provides prostheses, installation tools, and methods designed to replace natural facet joints at virtually all spinal levels including L1-L2, L2-L3, L3-L4, L4-L5, L5-S1, T-11-T12, and T12-L1. The prostheses, installation tools, and methods can restore a desired anatomy to a spine and give back to an individual a desired range of relative vertebral motion. The prostheses, installation tools, and methods also can lessen or alleviate spinal pain by relieving the source of nerve compression or impingement.

For the sake of description, the prostheses that embody features of the invention will be called either "cephalad" or "caudal" with relation to the portion of a given natural facet joint they replace. As previously described, a given natural facet joint has a superior half and an inferior half. In anatomical terms, the superior half of the joint is formed by the vertebral level below the joint (which can thus be called the caudal portion of the facet joint, i.e., because it is near the feet). The inferior half of the joint is formed by the vertebral level above the joint (which can thus be called the cephalad portion of the facet joint, i.e., because it is near the head). Thus, a prosthesis that, in use, replaces the caudal portion of a facet joint (i.e., the superior half) will be called a "caudal" prosthesis. Likewise, a prosthesis that, in use, replaces the cephalad portion of a facet joint (i.e., the inferior half) will be called a "cephalad" prosthesis.

One aspect of the invention provides a prosthesis to replace a cephalad portion of a natural facet joint on a vertebra. The prosthesis includes: an artificial facet joint bearing element adapted and

configured to replace the cephalad portion of the natural facet joint; and a fixation mechanism (such as a clamp) adapted and configured to attach the artificial facet joint bearing element to the vertebra, the fixation mechanism including a non-invasive support member adapted and configured to attach to a lamina portion of the vertebra, such as substantially at a spinous process location. The support member may be further adapted and configured to be in contact with the lamina portion of the vertebra on at least two opposing sides and possibly four surfaces of the lamina portion of the vertebra. The fixation mechanism is preferably further adapted and configured to attach the artificial facet joint element to the vertebra without blocking access to a pedicle portion of the vertebra.

In some embodiments the support member includes first and second vertebra contact surfaces, the distance between the first and second vertebra contact surfaces being adjustable. At least one of the first and second vertebral contact components may be movable with respect to the other vertebral contact component.

The prosthesis may also include an attachment mechanism attaching the artificial facet joint bearing element to the fixation mechanism. The attachment mechanism may traverse a midline of the vertebra. The attachment mechanism may be adapted and configured such that the artificial facet joint bearing element is movable in a cephalad or caudad direction with respect to the fixation mechanism. In some embodiments the attachment element includes a location element movable in a cephalad or caudad direction with respect to the fixation mechanism.

2....

In some embodiments the artificial facet joint bearing element is a right artificial facet joint bearing element and the natural facet joint is a right natural facet joint, and the prosthesis further includes a left artificial facet joint bearing element adapted and configured to replace a cephalad portion of a left natural facet joint. The right and left artificial facet joint bearing elements may be attached to the attachment element.

Another aspect of the invention provides a prosthesis to replace a cephalad portion of a natural facet joint on a vertebra, including an artificial facet joint bearing element adapted and configured to replace the cephalad portion of the natural facet joint; and a fixation mechanism (such as a clamp) adapted and configured to attach the artificial facet joint bearing element to the vertebra (such as a lamina portion of the vertebra) without penetrating any bone portion of the vertebra. In some embodiments the fixation mechanism may be adapted and configured to be in

contact with the attachment portion of the vertebra on at least two opposing sides, and possibly on four surfaces, of the vertebra. The fixation mechanism is preferably further adapted and configured to attach the artificial facet joint element to the vertebra without blocking access to a pedicle portion of the vertebra.

In some embodiments, the fixation mechanism includes first and second vertebra contact surfaces, the distance between the first and second vertebra contact surfaces being adjustable, such as by moving one of first and second vertebral contact components with respect to the other vertebral contact component.

The prosthesis may include an attachment mechanism attaching the artificial facet joint bearing element to the fixation mechanism. In some embodiments, the attachment mechanism disposes the artificial facet joint bearing element caudad from the fixation mechanism. In one embodiment the attachment mechanism traverses a midline of the vertebra. The attachment mechanism may be adapted and configured such that the artificial facet joint bearing element is movable in a cephalad or caudad direction with respect to the fixation mechanism. In some embodiments the fixation mechanism is a first fixation mechanism and the attachment mechanism is adapted and configured to penetrate a bone portion of the vertebra to form a second fixation mechanism attaching the artificial bearing element to the vertebra.

In some embodiments, the artificial facet joint bearing element is a right artificial facet joint bearing element and the natural facet joint is a right natural facet joint, with the prosthesis further including a left artificial facet joint bearing element adapted and configured to replace a cephalad portion of a left natural facet joint.

Another aspect of the invention provides a prosthesis to replace a cephalad portion of a natural facet joint on a vertebra, the prosthesis including an artificial facet joint bearing element adapted and configured to replace the cephalad portion of the natural facet joint; and means for affixing the artificial facet joint bearing element to the vertebra (such as a lamina portion of the vertebra) without penetrating any bone portion of the vertebra. In some embodiments, the means for affixing includes first and second components movable with respect to each other. The prosthesis according to this aspect of the invention may also include means for moving the artificial facet joint bearing element in cephalad and caudad directions with respect to the means for affixing.

In some embodiments, the artificial facet joint bearing element is a right artificial facet joint bearing element and the natural facet joint

is a right natural facet joint, with the prosthesis further including a left artificial facet joint bearing element adapted and configured to replace a cephalad portion of a left natural facet joint, and with the means for affixing including means for affixing the right and left artificial facet joint bearing elements to the vertebra. The prosthesis may also include means for moving the right and left artificial facet joint bearing elements in cephalad and caudad directions with respect to the means for affixing. In some embodiments, the prosthesis may also include means for affixing the artificial facet joint bearing element to the vertebra by penetrating a bone portion of the vertebra.

Another aspect of the invention provides a prosthesis to replace right and left cephalad portions of right and left natural facet joints on a vertebra, with the prosthesis including right and left artificial facet joint bearing elements adapted and configured to replace the cephalad portions of the right and left natural facet joints; and a fixation mechanism adapted and configured to attach the artificial facet joint bearing element to a lamina portion of the vertebra without penetrating any bone portion of the vertebra. The prosthesis may also include an attachment mechanism attaching the right and left artificial facet joint bearing elements to the fixation mechanism. The attachment mechanism may be adapted and configured to move the right and left artificial joint bearing elements in a cephalad or caudad direction with respect to the fixation mechanism.

Ŷ.

1787 T

Yet another aspect of the invention provides a method for implanting a cephalad facet joint prosthesis on a vertebra, with the method including the steps of affixing a fixation element to the vertebra (such as a lamina portion of the vertebra) without penetrating any bone portion of the vertebra; and disposing an artificial facet joint bearing element in a predetermined position with respect to the vertebra. In some embodiments the affixing step may include placing a fixation mechanism in contact with an attachment portion of the vertebra on at least two opposing sides of the attachment portion of the vertebra, such as by placing the fixation mechanism in contact with the attachment portion of the vertebra on four surfaces of the attachment portion of the vertebra. The fixation mechanism may include first and second vertebral contact components, with the affixing step including moving one of the first and second vertebral contact components with respect to the other. The affixing step may also include the step of preventing relative movement. between the first and second vertebral contact components after the moving step. In some embodiments the affixing step includes affixing a

fixation mechanism to the vertebra without blocking access to a pedicle portion of the vertebra.

The disposing step of this aspect of the invention may include fastening the artificial facet joint bearing element to a fixation mechanism, such as by inserting a fastener through the fixation element. The disposing step may also include moving the artificial facet joint bearing element in a cephalad or caudad direction with respect to the vertebra.

In this method, the fixation mechanism may be a first fixation mechanism, with the method further including the step of affixing a second fixation mechanism to the vertebra by penetrating the vertebra (such as by inserting a fastener into a lamina portion of the vertebra) and possibly attaching the second fixation mechanism to the first fixation mechanism. The fastener may be inserted through the fixation element across a midline of the vertebra, and the artificial facet joint bearing element may be attached to the fastener.

In some embodiments of the method, the artificial facet joint bearing element is a right artificial facet joint bearing element, with the disposing step further including disposing a left artificial facet joint bearing element in a predetermined position with respect to the vertebra.

Other features and advantages of the inventions are set forth in the following Description and Drawings, as well as in the appended Claims. Description of the Drawings

Figure 1 is a lateral elevation view of a normal human spinal column;

Figure 2 is a superior view of a normal human lumbar vertebra;

Figure 3 is a lateral elevation view of a vertebral lumbar facet joint;

Figure 4 is a posterior view of an artificial facet joint prosthesis installed in a patient according to one embodiment of this invention;

Figure 5 is a left side view of the embodiment of Figure 4, as installed in a patient:

Figure 6 is yet another view of the embodiment of Figure 4, as installed in a patient;

Figure 7 is a top view of the artificial facet joint prosthesis of the embodiment of Figure 4;

Figure 8 is a left view of the artificial facet joint prosthesis of the embodiment of Figure 4;

Figure 9 is a posterior view of the artificial facet joint

prosthesis of the embodiment of Figure 4;

Figure 10 is an anterior view of the artificial facet joint prosthesis of the embodiment of Figure 4;

Figure 11 is a bottom view of the artificial facet joint prosthesis of the embodiment of Figure 4;

Figure 12 is an exploded view of part of the cephalad portion of the artificial facet joint prosthesis of the embodiment of Figure 4;

Figure 13 is an artificial facet joint prosthesis according to another embodiment of this invention;

Figure 14 is a top view of the artificial facet joint prosthesis of the embodiment of Figure 13;

Figure 15 is a posterior view of the artificial facet joint prosthesis of the embodiment of Figure 13;

Figure 16 is a left side view of the artificial facet joint prosthesis of the embodiment of Figure 13;

Figure 17 is a posterior view of the caudal portion of the artificial facet joint prosthesis of the embodiment of Figure 13;

Figure 18 is a view of the cephalad bearing elements of the artificial facet joint prosthesis of the embodiment of Figure 13;

Figure 19 is an exploded view of a clamp assembly according to the embodiment of Figure 13; and

- 1

Figure 20 is a cross-sectional view of the clamp assembly of Figure 19.

The invention may be embodied in several forms without departing from its spirit or essential characteristics. The scope of the invention is defined in the appended claims, rather than in the specific description preceding them. All embodiments that fall within the meaning and range of equivalency of the claims are therefore intended to be embraced by the claims.

Detailed Description

Although the disclosure hereof is detailed and exact to enable those skilled in the art to practice the invention, the physical embodiments herein disclosed merely exemplify the invention that may be embodied in other specific structure. While the preferred embodiment has been described, the details may be changed without departing from the invention, which is defined by the claims.

Figures 4-12 show artificial cephalad and caudal facet joint prostheses for replacing a natural facet joint according to one aspect of the invention. The cephalad prosthesis has a bearing element 38 with a bearing surface 40. In this embodiment, bearing surface 40 has a convex

shape. Bearing element 38 and bearing surface 40 may be formed from biocompatible metals (such as cobalt chromium steel, surgical steels, titanium, titanium alloys, tantalum, tantalum alloys, aluminum, etc.), ceramics, polyethylene, biocompatible polymers, and other materials known in the prosthetic arts.

Depending on the patient's disease state, the condition of the patient's natural facet joint—including the facet joint's strength, location and orientation—may not be acceptable. As shown in Figures 4 and 5, therefore, the natural cephalad and caudal facet joint surfaces and the spinous process of vertebra 60 have been removed to enable the installation of a prosthetic facet joint without limitations presented by remaining portions of the natural facet joint. Other portions of the vertebra may be removed as required by the pathology of the patient's vertebra (e).

A fixation mechanism attaches the cephalad prosthesis to vertebra 60. In this embodiment of the invention, the fixation mechanism includes a non-invasive support member such as a two-part clamp formed from an upper clamp member 36 and a lower clamp member 41. Upper clamp member 36 has a hook with a cephalad directed portion 51, an anteriorly directed portion 37 and a caudad directed portion 39. The anterior surface of cephalad directed portion 51, the bottom surface of anteriorly directed portion 37 and the posterior surface of caudad directed portion 39 are in contact with a contact portion of the patient's vertebra, shown as lamina portion 62 in Figures 4 and 5. Likewise, lower clamp member 41 has an anteriorly directed portion 42 and a cephalad directed portion 43. The top surface of anteriorly directed portion 42 and the posterior surface of cephalad directed portion 43 are also in contact with the contact portion of the vertebra, such as lamina portion 62 in Figures 4 and 5.

In this embodiment, the fixation mechanism of the cephalad prosthesis attaches to the lamina of vertebra 60 after removal of the spinous process from that vertebra. In other embodiments, the fixation mechanism may come in contact with other parts of the vertebra and at fewer than four contact points, such as by contacting two opposing sides of the vertebral contact portion. In addition, in other embodiments it may not be necessary to first remove the spinous process.

For purposes of installation and to conform most closely with the patient's anatomy, upper and lower clamp members 36 and 41 are movable with respect to each other. As shown in Figure 12, a posterior cephalad directed portion 44 of clamp member 41 slides in a slot 45 formed posterior to a body portion 46 of upper clamp member 36. After placing

upper clamp member 36 on contact portion 62 of vertebra 60, lower clamp member 41 may be slid upwards until it makes firm contact with contact portion 62 as well. A set screw 47 may be advanced within interior threads 48 formed in the posterior portion of upper clamp member 36 to firmly contact lower clamp member 41 to hold it in place. A nut 49 is then advanced onto exterior threads 50 formed in the posterior portion of upper clamp member 36 to lock set screw 47 and lower clamp member 41 in place.

The cephalad facet joint bearing elements 38 are attached to the assembly via an attachment mechanism. In the embodiment of Figures 4-12, the attachment mechanism includes fasteners such as screws 63 inserted through the body portion 46 of upper clamp member 36 into a hole formed in each bearing element 38. The angle in which screws 63 are inserted (and, therefore the relative orientation of the cephalad and caudal facet joint bearing elements) may be determined using tools such as those described in copending U.S. Patent Application Serial No. 10/438,294 entitled "Prostheses, Tools and Methods for Replacement of Natural Facet Joints With Artificial Facet Joint Surfaces," filed May 14, 2003, the disclosure of which is incorporated herein by reference. As shown in Figures 4 and 5, if enough bone around the lamina portion of vertebra 60 is left intact, screws 63 may penetrate the lamina to form an additional fixation mechanism.

17

In an alternative embodiment, because of the amount of bone removed from the patient's vertebra prior to installation of the prosthesis, the attachment mechanism does not penetrate the bone. In this embodiment, the fasteners such as screws 63 are inserted through the body portion 46 of upper clamp member 36 into a threaded hole formed in each bearing element 38 but do not extend through the lamina or any other portion of the vertebra. As in the other embodiment, screws 63 traverse the midline of vertebra 60 and extend caudad from the clamp to provide the bearing element orientation shown. Other orientations of attachment mechanisms are possible, of course. In addition, the location of bearing elements 38 (i.e., in cephalad/caudad directions, left/right, etc.) may be adjusted by using different size or shape fasteners.

The artificial cephalad facet joint prosthesis of Figures 4-12 may be used with any suitable natural or artificial caudal facet joint members. Figures 4-12 show one suitable artificial caudal facet joint prosthesis that may be used. The caudal prosthesis has a bearing element 52 with a bearing surface 54. In this embodiment, bearing surface 54 is concave. Bearing element 52 may be formed from biocompatible metals (such

as cobalt chromium steel, surgical steels, titanium, titanium alloys, tantalum, tantalum alloys, aluminum, etc.), ceramics, polyethylene, biocompatible polymers, and other materials known in the prosthetic arts, and bearing surface 54 may be formed from biocompatible metals (such as cobalt chromium steel, surgical steels, titanium, titanium alloys, tantalum, tantalum alloys, aluminum, etc.), ceramics, polyethylene, biocompatible polymers, and other materials known in the prosthetic arts.

In one embodiment, the natural caudal facet surface has been removed, and fixation element 56 attaches the caudal prosthesis to a vertebra 70 via a pedicle in an orientation and position that places bearing surface 54 in approximately the same location as the natural facet joint surface the prosthesis replaces. In an alternative embodiment, the bearing surface 54 may be placed in a location different than the natural facet joint surface, either more medial or more lateral, more cephalad or more caudad, and/or rotated from the natural anatomical orientation and orientation. In addition, in other embodiments the caudal component can be attached to the vertebral body in addition to the pedicle or to the vertebral body alone.

As shown in the embodiment of Figures 4-12, fixation element 56 is a screw attached to bearing element 54 via a hole formed in bearing element 52 and is inserted into a pedicle portion 72 of vertebra 70. Other possible fixation elements include stems, corkscrews, wire, staples, adhesives, bone cements, and other materials known in the prosthetic arts. Fixation element 56 can also be inserted into the vertebral body in addition to or in place of the pedicle.

In this embodiment, bearing element 52 has a serrated fixation surface 57 adapted to contact a contact portion 74 of vertebra 70. This optional fixation surface 57 helps prevent rotation of the bearing element 52. In addition, fixation surface 57 may be coated with bone ingrowth material, and any optional serrations increase the surface area for bone ingrowth. Further details regarding the design and installation of this caudal prosthesis may be found in copending and commonly owned U.S. Patent Application Serial No. 10/438,294 entitled "Prostheses, Tools and Methods for Replacement of Natural Facet Joints With Artificial Facet Joint Surfaces," filed May 14, 2003.

Figures 13-20 show another embodiment of the artificial facet joint prosthesis of this invention for replacing a natural facet joint. The cephalad prosthesis has a bearing element 80 with a bearing surface 82. In this embodiment, bearing surface 82 has a convex shape. Bearing element 80 and bearing surface 82 may be formed from biocompatible metals

(such as cobalt chromium steel, surgical steels, titanium, titanium alloys, tantalum, tantalum alloys, aluminum, etc.), ceramics, polyethylene, biocompatible polymers, and other materials known in the prosthetic arts.

A fixation mechanism attaches the cephalad prosthesis to the vertebra. In this embodiment of the invention, the fixation mechanism includes a non-invasive support member such as a two-part clamp formed from an upper clamp member 84 and a lower clamp member 86. Upper clamp member 84 has a hook with a cephalad directed portion 88, an anteriorly directed portion 90 and a caudad directed portion 92. The anterior surface of cephalad directed portion 88, the bottom surface of anteriorly. directed portion 90 and the posterior surface of caudad directed portion 92 are in contact with a contact portion of the patient's vertebra (such as the lamina) when the prosthesis is installed in a patient. Likewise, lower clamp member 86 has a caudad directed portion 94, an anteriorly directed portion 96 and a cephalad directed portion 98. The anterior surface of caudad directed portion 94, the top surface of anteriorly directed portion 96 and the posterior surface of cephalad directed portion 98 are also in contact with the contact portion of the vertebra (such as the lamina) when the prosthesis is installed in a patient. This arrangement of upper and lower clamps provides for contact with the lamina (or other vertebra contact portion) on four sides.

In this embodiment, the fixation mechanism of the cephalad prosthesis attaches to the lamina of vertebra after removal of the spinous process from that vertebra. In other embodiments, the fixation mechanism may come in contact with other parts of the vertebra and at fewer than four contact points, such as by contacting two opposing sides of the vertebral contact portion. In addition, in other embodiments it may not be necessary to first remove the spinous process.

For purposes of installation and to conform most closely with the patient's anatomy, upper and lower clamp members 84 and 86 are movable with respect to each other. As shown in Figures 19 and 20, a posterior cephalad directed portion 100 of clamp member 86 slides in a slot 102 formed in a body portion 104 of upper clamp member 84. As shown, slot 102 places clamp member portion 100 at a 15° angle from vertical, and a shim 106 is placed posterior to clamp member portion 100. This orientation may be changed, of course, to meet the needs of the patient's anatomy.

After placing upper clamp member 84 on the contact portion of the vertebra, lower clamp member 86 may be slid upwards until it makes firm contact with the contact portion as well. A set screw 108 is then

advanced within interior threads 110 formed in body portion 104 of upper clamp member 84 to firmly contact lower clamp member 86 to hold it in place.

The cephalad facet joint bearing elements 80 are attached to the assembly via an attachment mechanism, including a movable location element for adjusting the location of bearing elements 80. In this embodiment, the location element includes a rod 112 to which bearing elements 80 are attached via attachment wings 113. During installation, rod 112 is movable in a space formed by a pair of inserts 114 and 116 to adjust the location of bearing elements 80. Once the location has been set, inserts 114 and 116 are tightened against rod 112 by advancing a second set screw 118 against insert 116 via internal threads 120 formed in the body portion of the upper clamp member. A nut 122 is then advanced onto exterior threads 124 formed in the body portion of upper clamp member 84 to the other components in place.

The artificial cephalad facet joint prosthesis of Figures 13-16 and 18-20 may be used with any suitable natural or artificial caudal facet joint members. Figures 13-17 show one suitable artificial caudal facet joint prosthesis that may be used. The caudal prosthesis has a bearing element 130 with a bearing surface 132. In this embodiment, bearing surface 132 is concave. Bearing element 130 and bearing surface 132 may be formed from biocompatible metals (such as cobalt chromium steel, surgical steels, titanium, titanium alloys, tantalum, tantalum alloys, aluminum, etc.), ceramics, polyethylene, biocompatible polymers, and other materials known in the prosthetic arts.

To install the artificial caudal prosthesis of this embodiment, the natural caudal facet surface is removed, and a fixation element (such as a screw) is inserted through holes 134 formed in arms 136 extending from bearing elements 130 into pedicle portions of a vertebra to attach the caudal prosthesis to the vertebra in an orientation and position that places bearing surface 132 in approximately the same location as the natural facet joint surface the prosthesis replaces. The spacing between bearing elements 130 is set by a bar 138. In an alternative embodiment, the bearing surface may be placed in a location different than the natural facet joint surface, either more medial or more lateral, more cephalad or more caudad, and/or rotated from the natural anatomical orientation. In addition, in other embodiments the caudal component can be attached to the vertebral body in addition to the pedicle or to the vertebral body alone. Other possible fixation elements include stems, corkscrews, wire, staples, adhesives, bone cements, and other materials

known in the prosthetic arts.

As shown in the preceding embodiments of the invention, unlike other facet joint prostheses that attach to the pedicle, the use of one or more posterior elements of the vertebra to attach the cephalad facet joint prosthesis of this invention does not block access to the pedicle area, leaving this area free to be used to attach other prostheses or devices. Other embodiments of the invention may block the pedicle area, of course, without departing from the scope or spirit of the invention. Also, in some embodiments, the entire prosthesis other than the bearing surface may be coated with bone ingrowth material.

The above described embodiments of this invention are merely descriptive of its principles and are not to be limited. The scope of this invention instead shall be determined from the scope of the following claims, including their equivalents.

What is claimed is:

1. A prosthesis to replace a cephalad portion of a natural facet joint on a vertebra, the prosthesis comprising:

an artificial facet joint bearing element adapted and configured to replace the cephalad portion of the natural facet joint; and

- a fixation mechanism adapted and configured to attach the artificial facet joint bearing element to the vertebra without penetrating any bone portion of the vertebra.
- 2. The prosthesis of claim 1 wherein the fixation mechanism is further adapted and configured to attach to a lamina portion of the vertebra.
- 3. The prosthesis of claim 2 wherein the fixation mechanism is further adapted and configured to attach to the lamina portion of the vertebra substantially at a spinous process location.
- 4. The prosthesis of claim 3 wherein the fixation mechanism is further adapted and configured to be in contact with the lamina portion of the vertebra on at least two opposing sides of the lamina portion of the vertebra.
- 5. The prosthesis of claim 4 wherein the fixation mechanism is further adapted and configured to be in contact with the lamina portion of the vertebra on four surfaces of the lamina portion of the vertebra.
- 6. The prosthesis of claim 1 wherein the fixation mechanism is further adapted and configured to attach the artificial facet joint element to the vertebra without blocking access to a pedicle portion of the vertebra.
- 7. The prosthesis of claim 1 wherein the fixation mechanism is further adapted and configured to be in contact with an attachment portion of the vertebra on at least two opposing sides of the attachment portion of the vertebra.
- 8. The prosthesis of claim 7 wherein the fixation mechanism is further adapted and configured to be in contact with the attachment portion of the vertebra on four surfaces of the attachment portion of the vertebra.
- 9. The prosthesis of claim 1 wherein the fixation mechanism comprises first and second vertebra contact surfaces, the distance between the first and second vertebra contact surfaces being adjustable.
- 10. The prosthesis of claim 1 wherein the fixation mechanism comprises first and second vertebral contact components comprising first and second vertebral contact surfaces, respectively, at least one of the first and second vertebral contact components being movable with respect

to the other vertebral contact component.

11. The prosthesis of claim 1 further comprising an attachment mechanism attaching the artificial facet joint bearing element to the fixation mechanism.

- 12. The prosthesis of claim 11 wherein the attachment mechanism traverses a midline of the vertebra.
- 13. The prosthesis of claim 11 wherein the attachment mechanism is a screw.
- 14. The prosthesis of claim 11 wherein the fixation mechanism is a first fixation mechanism and wherein the attachment mechanism is adapted and configured to penetrate a bone portion of the vertebra to form a second fixation mechanism attaching the artificial bearing element to the vertebra.
- 15. The prosthesis of claim 11 wherein the attachment mechanism disposes the artificial facet joint bearing element caudad from the fixation mechanism.
- 16. The prosthesis of claim 11 wherein the attachment mechanism is adapted and configured such that the artificial facet joint bearing element is movable in a cephalad or caudad direction with respect to the fixation mechanism.
- 17. The prosthesis of claim 16 wherein the attachment element comprises a location element movable in a cephalad or caudad direction with respect to the fixation mechanism.
- 18. The prosthesis of claim 17 wherein the artificial facet joint bearing element is a right artificial facet joint bearing element and the natural facet joint is a right natural facet joint, the prosthesis further comprising a left artificial facet joint bearing element adapted and configured to replace a cephalad portion of a left natural facet joint.
- 19. The prosthesis of claim 18 wherein the right and left artificial facet joint bearing elements are attached to the attachment element.
- 20. The prosthesis of claim 1 wherein the artificial facet joint bearing element is a right artificial facet joint bearing element and the natural facet joint is a right natural facet joint, the prosthesis further comprising a left artificial facet joint bearing element adapted and configured to replace a cephalad portion of a left natural facet joint.
- 21. The prosthesis of claim 20 further comprising right and left attachment elements attaching the right and left artificial facet joint

bearing elements to the fixation mechanism.

22. The prosthesis of claim 1 wherein the fixation mechanism comprises a clamp.

- 23. The prosthesis of claim 1 wherein the fixation mechanism is a first fixation mechanism, the prosthesis comprising a second fixation mechanism adapted and configured to penetrate a bone portion of the vertebra to attach the artificial bearing element to the vertebra.
- 24. A prosthesis to replace right and left cephalad portions of right and left natural facet joints on a vertebra, the prosthesis comprising:

right and left artificial facet joint bearing elements adapted and configured to replace the cephalad portions of the right and left natural facet joints; and

- a fixation mechanism adapted and configured to attach the artificial facet joint bearing element to a lamina portion of the vertebra without penetrating any bone portion of the vertebra.
- 25. The prosthesis of claim 24 further comprising an attachment mechanism attaching the right and left artificial facet joint bearing elements to the fixation mechanism.
- 26. The prosthesis of claim 25 wherein the attachment mechanism is adapted and configured to move the right and left artificial joint bearing elements in a cephalad or caudad direction with respect to the fixation mechanism.
- 27. The prosthesis of claim 25 wherein the attachment mechanism comprises a rod.
- 28. The prosthesis of claim 25 wherein the attachment mechanism comprises right and left fasteners for the right and left artificial facet joint bearing elements, respectively.
- 29. A prosthesis to replace a cephalad portion of a natural facet joint on a vertebra, the prosthesis comprising:

an artificial facet joint bearing element adapted and configured to replace the cephalad portion of the natural facet joint; and

- a fixation mechanism adapted and configured to attach the artificial facet joint bearing element to the vertebra, the fixation mechanism comprising a non-invasive support member adapted and configured to attach to a lamina portion of the vertebra.
- 30. The prosthesis of claim 29 wherein the support member is further adapted and configured to attach to the lamina portion of the vertebra substantially at a spinous process location.
 - 31. The prosthesis of claim 30 wherein the support member is

further adapted and configured to be in contact with the lamina portion of the vertebra on at least two opposing sides of the lamina portion of the vertebra.

- 32. The prosthesis of claim 31 wherein the support member is further adapted and configured to be in contact with the lamina portion of the vertebra on four surfaces of the lamina portion of the vertebra.
- 33. The prosthesis of claim 29 wherein the fixation mechanism is further adapted and configured to attach the artificial facet joint element to the vertebra without blocking access to a pedicle portion of the vertebra.
- 34. The prosthesis of claim 29 wherein the support member comprises first and second vertebra contact surfaces, the distance between the first and second vertebra contact surfaces being adjustable.
- 35. The prosthesis of claim 29 wherein the support member comprises first and second vertebral contact components comprising first and second vertebral contact surfaces, respectively, at least one of the first and second vertebral contact components being movable with respect to the other vertebral contact component.
- 36. The prosthesis of claim 29 further comprising an attachment mechanism attaching the artificial facet joint bearing element to the fixation mechanism.
- 37. The prosthesis of claim 36 wherein the attachment mechanism traverses a midline of the vertebra.
- 38. The prosthesis of claim 36 wherein the attachment mechanism is a screw.
- 39. The prosthesis of claim 36 wherein the attachment mechanism disposes the artificial facet joint bearing element caudad from the fixation mechanism.
- 40. The prosthesis of claim 36 wherein the attachment mechanism is adapted and configured such that the artificial facet joint bearing element is movable in a cephalad or caudad direction with respect to the fixation mechanism.
- 41. The prosthesis of claim 40 wherein the attachment element comprises a location element movable in a cephalad or caudad direction with respect to the fixation mechanism.
- 42. The prosthesis of claim 41 wherein the artificial facet joint bearing element is a right artificial facet joint bearing element and the natural facet joint is a right natural facet joint, the prosthesis further comprising a left artificial facet joint bearing element adapted and configured to replace a cephalad portion of a left natural facet

joint.

43. The prosthesis of claim 42 wherein the right and left artificial facet joint bearing elements are attached to the attachment element.

- 44. The prosthesis of claim 29 wherein the artificial facet joint bearing element is a right artificial facet joint bearing element and the natural facet joint is a right natural facet joint, the prosthesis further comprising a left artificial facet joint bearing element adapted and configured to replace a cephalad portion of a left natural facet joint.
- 45. The prosthesis of claim 44 further comprising right and left attachment elements attaching the right and left artificial facet joint bearing elements to the fixation mechanism.
- 46. The prosthesis of claim 29 wherein the fixation mechanism comprises a clamp.

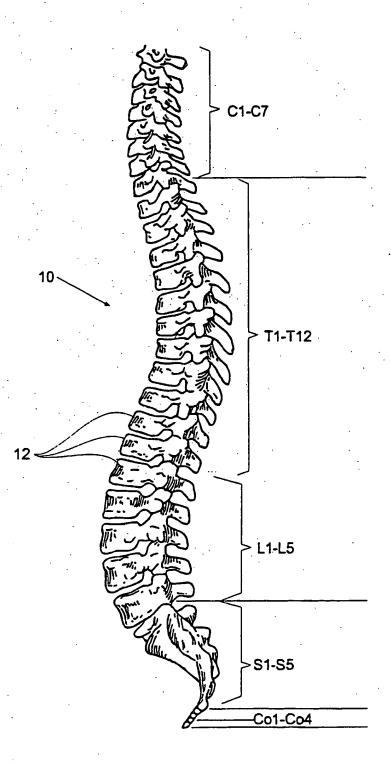
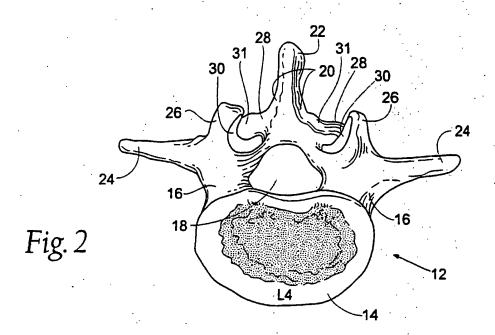
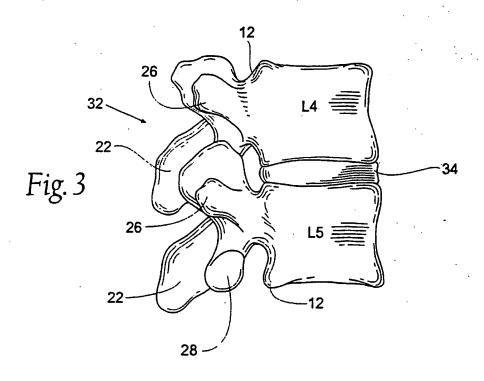


Fig. I





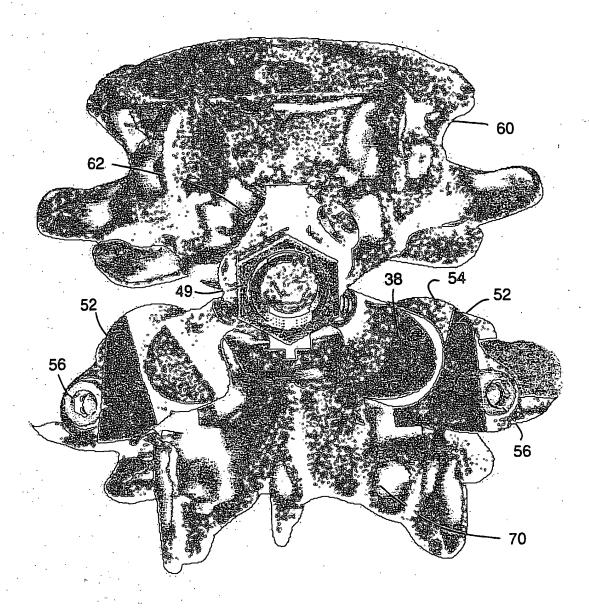


Fig. 4

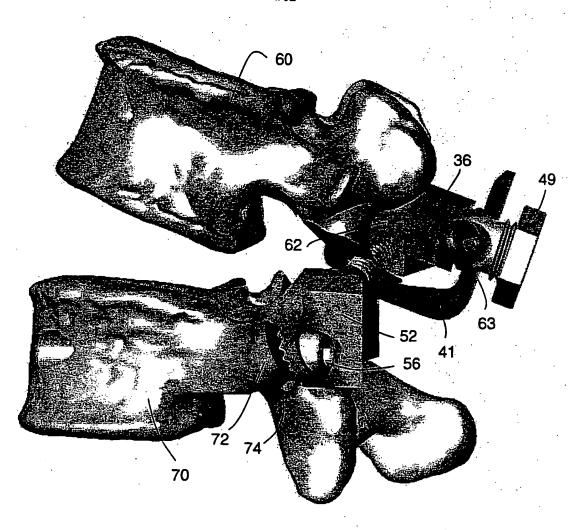


Fig. 5

5/12.

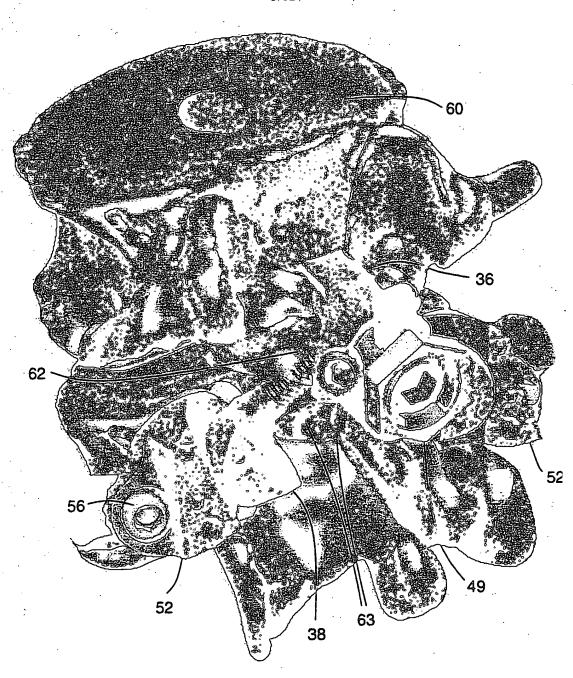
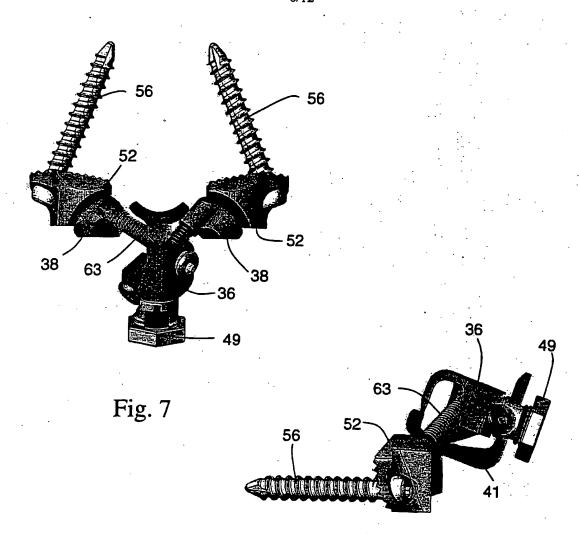


Fig. 6



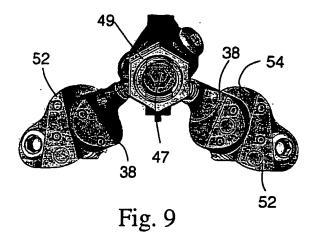


Fig. 8

WO 2005/009301

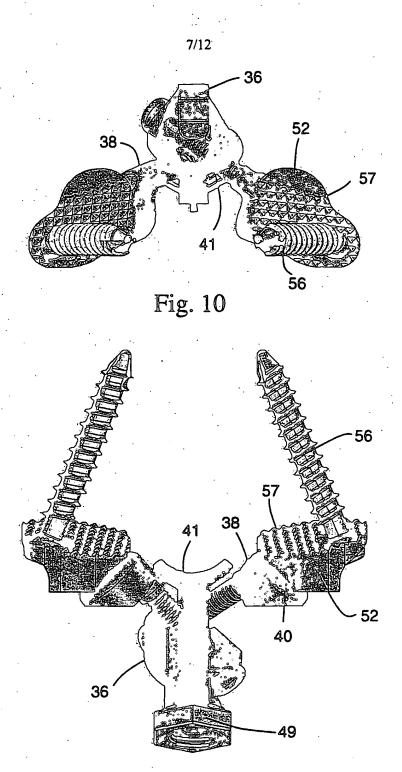


Fig. 11

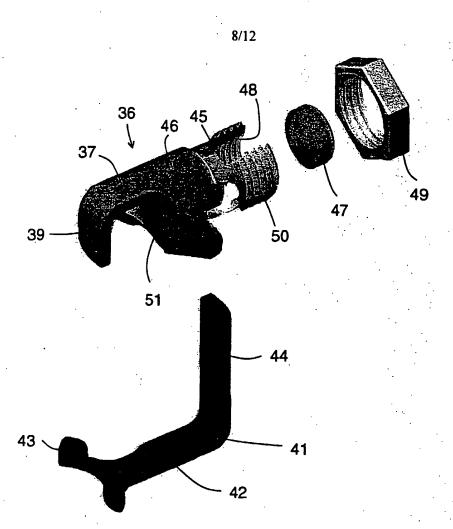


Fig. 12

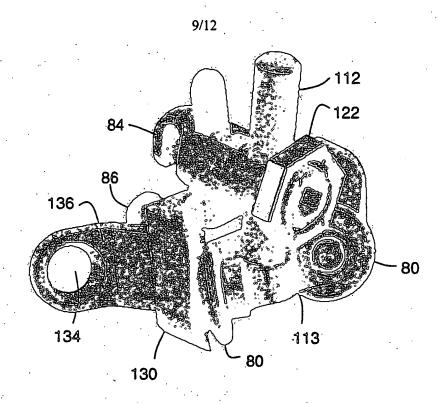
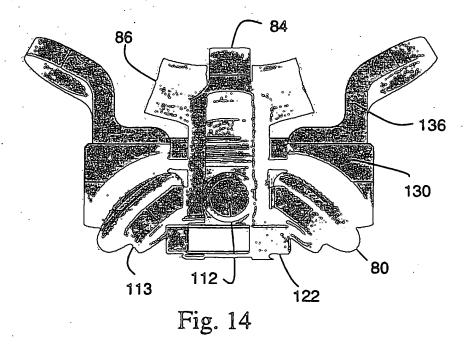


Fig. 13



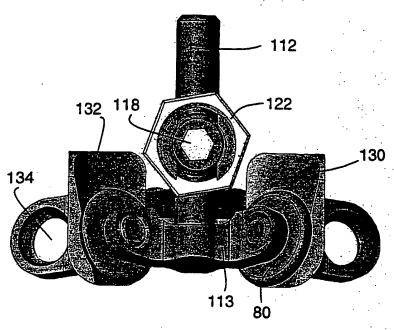


Fig. 15

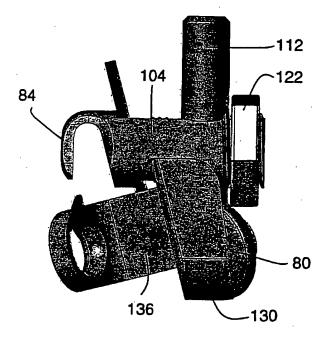


Fig. 16

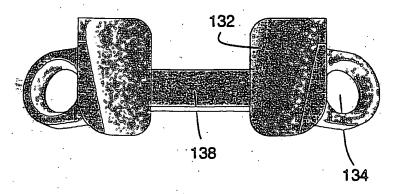


Fig. 17

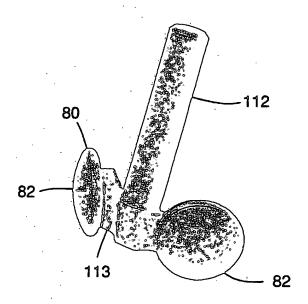
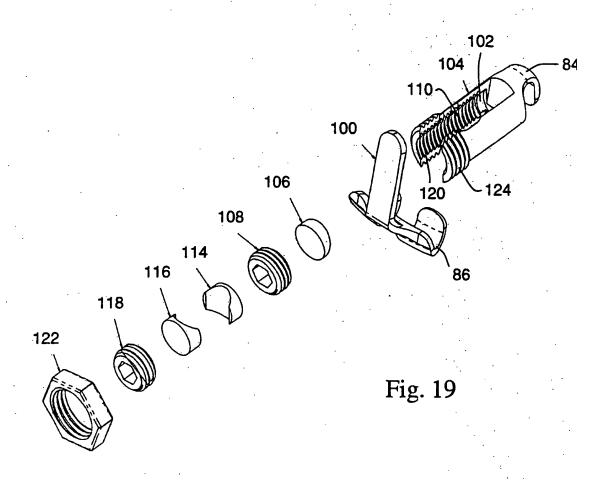


Fig. 18



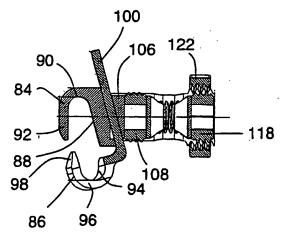


Fig. 20

INTERNATIONAL SEARCH REPORT

International Application No PUS2004/016774

			1 64 / 032004	7010774	
A. CLASSI IPC 7	FICATION OF SUBJECT MATTER A61F2/44				
According to	o International Patent Classification (IPC) or to both national class	ification and IPC			
	SEARCHED				
Minimum do	ocumentation searched (classification system followed by classific	ation symbols)		***	
IPC 7	A61F				
Documentat	ion searched other than minimum documentation to the extent that	Il such documents are incli	uded in the fields sea	rched	
Electronic de					
	ata base consulted during the international search (name of data	base and, where practical	, searchiterins used)		
EPO-Int	ternal				
		•			
C. DOCUME	INTS CONSIDERED TO BE RELEVANT				
Category °	Citation of document, with indication, where appropriate, of the	relevant passages	· I	Relevant to claim No.	
•				TIDIOVANI IO CAGNITIVO.	
x I	US 6 132 464 A (MARTIN JEAN-RAY)	MOND)		1-4,6-8,	
	17 October 2000 (2000-10-17)	iono) .		11,13,	
I				15,	
				20-22,	
				24,25,	
				29,30,	
1				36,38, 39,44-46	
	claims 1,3; figures			39,44-40	
	column 6, line 19 - column 7, li	ine 54			
Α]				14,23,28	
**		,		1.	
		-/	-		
	The end		.		
			İ	·	
′ 1				•	
			į		
<u> </u>	er documents are listed in the continuation of box C.	Patent family m	nembers are listed in a	innex.	
	egories of cited documents :	"T" later document publi	ished after the interne	ational filing date	
"A" documen consider	It defining the general state of the art which is not red to be of particular relevance	cited to understand	not in conflict with the the principle or theor	y underlying the	
"E" eartier do fiting dal	ocument but published on or after the international	"X" document of particul	lar relevance; the clair	med invention	
"L" document	t which may throw doubts on priority claim(s) or clied to establish the publication date of another	involve an inventive	e step when the docur	considered to ment is taken alone	
citation	med invention nitive step when the				
other me	nt referring to an oral disclosure, use, exhibition or eans	COCCURRENT IS CONTEST	ned with one or more nation being obvious t	OTHER SUCH COCU.	
P° documen later tha	It published prior to the international filing date but in the priority date claimed	in the art. *8* document member of			
Date of the ac	ctual completion of the international search		e international search		
16	September 2004	23/09/20	23/09/2004		
Name and ma	alling address of the ISA	Authorized officer			
	European Patent Office, P.B. 5618 Patentiaan 2 NL - 2280 HV Rijswijk		•	1	
	Tel. (+31-70) 340-2040, Tx. 31 651 epo nl. Fax: (+31-70) 340-3016	Stach, R	t		

INTERNATIONAL SEARCH REPORT

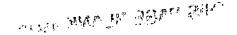
International Application No PC/US2004/016774

		PS/US2004/016774
	STOR) DOCUMENTS CONSIDERED TO BE RELEVANT	
Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 5 571 191 A (FITZ WILLIAM R) 5 November 1996 (1996-11-05) claim 1; figures 1-3 column 2, line 61 - column 3, line 25	1,6-8, 20,29,44
A		14,15, 18,24, 33,43
Α .	WO 02/065954 A (BORSCHNECK DANIEL P; SAUNDERS GERALD A B (CA); UNIV KINGSTON (CA); SO) 29 August 2002 (2002-08-29)	1,6,7, 9-11,13, 14,16, 17,23, 24,29, 33-36, 38,40
	claims 1,12,13,17; figures 3f-7b page 8, line 5 - page 9, line 15	30,40
		·
	·	
		·

INTERNATIONAL SEARCH REPORT

International Application No PS/US2004/016774

					/ US20U4/ U16//4
Patent document cited in search report		Publication date		Patent family member(s)	Publication date
US 6132464	A .	17-10-2000	FR AT AU CA DE EP WO	2721501 A1 173601 T 2797095 A 2193697 A1 69506254 D1 0767637 A1 9600049 A1	29-12-1995 15-12-1998 19-01-1996 04-01-1996 07-01-1999 16-04-1997 04-01-1996
US 5571191	Α	05-11-1996	US	RE36758 E	27-06-2000
WO 02065954	Α	29-08-2002	WO CA US	02065954 A1 2437575 A1 2002151895 A1	29-08-2002 29-08-2002 17-10-2002



THIS PAGE BLANK (USPTO)

This Page is Inserted by IFW Indexing and Scanning Operations and is not part of the Official Record

BEST AVAILABLE IMAGES

Defective images within this document are accurate representations of the original documents submitted by the applicant.

Defects in the images include but are not limited to the items checked:

BLACK BORDERS

IMAGE CUT OFF AT TOP, BOTTOM OR SIDES

☐ FADED TEXT OR DRAWING
D BLURRED OR ILLEGIBLE TEXT OR DRAWING
☐ SKEWED/SLANTED IMAGES
☐ COLOR OR BLACK AND WHITE PHOTOGRAPHS
☐ GRAY SCALE DOCUMENTS
☐ LINES OR MARKS ON ORIGINAL DOCUMENT
☐ REFERENCE(S) OR EXHIBIT(S) SUBMITTED ARE POOR QUALITY
OTHER:

IMAGES ARE BEST AVAILABLE COPY.

As rescanning these documents will not correct the image problems checked, please do not report these problems to the IFW Image Problem Mailbox.

THIS PAGE BLANK (USPTO)